

DESCRIPTION

METHODS FOR ELECTRONIC FLUORESCENT
PERTURBATION FOR ANALYSIS AND ELECTRONIC
PERTURBATION CATALYSIS FOR SYNTHESIS

Field of the Invention

This invention relates to systems, devices, methods, and mechanisms for performing multi-step molecular biological analysis, nucleic acid hybridization reactions, nucleic acid sequencing, and the catalysis of biomolecular, organic and inorganic reactions. More particularly, the molecular biological type analysis involves electronic fluorescent perturbation mechanisms for the detection of DNA hybrids, point mutations, deletions or repeating sequences in nucleic acid hybridization reactions, electronic fluorescent perturbation mechanisms for sequencing of DNA and RNA molecules, and electric field based catalytic mechanisms for biomolecular, biopolymer and other chemical reactions.

Related Application Information

This application is a continuation application of Application Serial No. 08/496,864, filed February 2, 2000, which is a continuation application of Application Serial No. 08/855,058, filed May 14, 1997, entitled "Methods for Electronic Fluorescent Perturbation for Analysis and electronic Perturbation Catalysis for Synthesis," issued as U.S. Patent No. 6,048,690, which is a continuation-in-part application of Application Serial No. 08/534,454, filed September 27, 1995, entitled "Methods for Hybridization Analysis Utilizing Electrically Controlled Hybridization", now issued as U.S. Patent No. 5,849,486, all of which are incorporated herein by reference as if fully set forth herein.

Background of the Invention

Molecular biology comprises a wide variety of techniques for the analysis of nucleic acid and protein. Many of these techniques and procedures form the basis of clinical diagnostic assays and tests. These techniques include nucleic acid hybridization analysis, restriction enzyme analysis, genetic sequence analysis, and the separation and purification of nucleic acids and proteins (See, e.g., J. Sambrook, E. F. Fritsch, and T. Maniatis, *Molecular*

1 Cloning: A Laboratory Manual, 2 Ed., Cold spring Harbor Laboratory Press, Cold Spring
2 Harbor, New York, 1989).

3 Most of these techniques involve carrying out numerous operations (e.g., pipetting,
4 centrifugations, electrophoresis) on a large number of samples. They are often complex and
5 time consuming, and generally require a high degree of accuracy. Many a technique is
6 limited in its application by a lack of sensitivity, specificity, or reproducibility. For example,
7 these problems have limited many diagnostic applications of nucleic acid hybridization
8 analysis.

9 The complete process for carrying out a DNA hybridization analysis for a genetic or
10 infectious disease is very involved. Broadly speaking, the complete process may be divided
11 into a number of steps and substeps. In the case of genetic disease diagnosis, the first step
12 involves obtaining the sample (blood or tissue). Depending on the type of sample, various
13 pre-treatments would be carried out. The second step involves disrupting or lysing the cells,
14 which then release the crude DNA material along with other cellular constituents. Generally,
15 several sub-steps are necessary to remove cell debris and to purify further the crude DNA. At
16 this point several options exist for further processing and analysis. One option involves
17 denaturing the purified sample DNA and carrying out a direct hybridization analysis in one of
18 many formats (dot blot, microbead, microliter plate, etc.). A second option, called Southern
19 blot hybridization, involves cleaving the DNA with restriction enzymes, separating the DNA
20 fragments on an electrophoretic gel, blotting to a membrane filter, and then hybridizing the
21 blot with specific DNA probe sequences. This procedure effectively reduces the complexity
22 of the genomic DNA sample, and thereby helps to improve the hybridization specificity and
23 sensitivity. Unfortunately, this procedure is long and arduous. A third option is to carry out
24 the polymerase chain reaction (PCR) or other amplification procedure. The PCR procedure
25 amplifies (increases) the number of target DNA sequences. Amplification of target DNA
26 helps to overcome problems related to complexity and sensitivity in genomic DNA analysis.
27 All these procedures are time consuming, relatively complicated, and add significantly to the
28 cost of a diagnostic test. After these sample preparation and DNA processing steps, the
29 actual hybridization reaction is performed. Finally, detection and data analysis convert the
30 hybridization event into an analytical result.

31 The steps of sample preparation and processing have typically been performed
32 separate and apart from the other main steps of hybridization and detection and analysis.

1 Indeed, the various substeps comprising sample preparation and DNA processing have often
2 been performed as a discrete operation separate and apart from the other substeps.
3 Considering these substeps in more detail, samples have been obtained through any number
4 of means, such as obtaining of full blood, tissue, or other biological fluid samples. In the
5 case of blood, the sample is processed to remove red blood cells and retain the desired
6 nucleated (white) cells. This process is usually carried out by density gradient centrifugation.
7 Cell disruption or lysis is then carried out, preferably by the technique of sonication,
8 freeze/thawing, or by addition of lysing reagents. Crude DNA is then separated from the
9 cellular debris by a centrifugation step. Prior to hybridization, double-stranded DNA is
10 denatured into single-stranded form. Denaturation of the double-stranded DNA has generally
11 been performed by the techniques involving heating ($>T_m$), changing salt concentration,
12 addition of base (NaOH), or denaturing reagents (urea, formamide, etc.). Workers have
13 suggested denaturing DNA into its single-stranded form in an electrochemical cell. The
14 theory is stated to be that there is electron transfer to the DNA at the interface of an electrode,
15 which effectively weakens the double-stranded structure and results in separation of the
16 strands. See, generally, Stanley, "DNA Denaturation by an Electric Potential", U.K. patent
17 application 2,247,889 published March 18, 1992.

18 Nucleic acid hybridization analysis generally involves the detection of a very small
19 number of specific target nucleic acids (DNA or RNA) with an excess of probe DNA, among
20 a relatively large amount of complex non-target nucleic acids. The substeps of DNA
21 complexity reduction in sample preparation have been utilized to help detect low copy
22 numbers (i.e. 10,000 to 100,000) of nucleic acid targets. DNA complexity is overcome to
23 some degree by amplification of target nucleic acid sequences using polymerase chain
24 reaction (PCR). (See, M.A. Innis et al, PCR Protocols: A Guide to Methods and
25 Applications, Academic Press, 1990). While amplification results in an enormous number of
26 target nucleic acid sequences that improves the subsequent direct probe hybridization step,
27 amplification involves lengthy and cumbersome procedures that typically must be performed
28 on a stand alone basis relative to the other substeps. Substantially complicated and relatively
29 large equipment is required to perform the amplification step.

30 The actual hybridization reaction represents the most important and central step in the
31 whole process. The hybridization step involves placing the prepared DNA sample in contact
32 with a specific reporter probe, at a set of optimal conditions for hybridization to occur to the

1 target DNA sequence. Hybridization may be performed in any one of a number of formats.
2 For example, multiple sample nucleic acid hybridization analysis has been conducted on a
3 variety of filter and solid support formats (See G. A. Beltz et al., in Methods in Enzymology,
4 Vol. 100, Part B, R. Wu, L. Grossman, K. Moldave, Eds., Academic Press, New York,
5 Chapter 19, pp. 266-308, 1985). One format, the so-called "dot blot" hybridization, involves
6 the non-covalent attachment of target DNAs to filter, which are subsequently hybridized with
7 a radioisotope labeled probe(s). "Dot blot" hybridization gained wide-spread use, and many
8 versions were developed (see M. L. M. Anderson and B. D. Young, in Nucleic Acid
9 Hybridization - A Practical Approach, B. D. Hames and S. J. Higgins, Eds., IRL Press,
10 Washington, D.C. Chapter 4, pp. 73-111, 1985). It has been developed for multiple analysis
11 of genomic mutations (D. Nanibhushan and D. Rabin, in EPA 0228075, July 8, 1987) and for
12 the detection of overlapping clones and the construction of genomic maps (G. A. Evans, in
13 US Patent Number 5,219,726, June 15, 1993).

14 New techniques are being developed for carrying out multiple sample nucleic acid
15 hybridization analysis on micro-formatted multiplex or matrix devices (e.g., DNA chips) (see
16 M. Barinaga, 253 Science, pp. 1489, 1991; W. Bains, 10 Bio/Technology, pp. 757-758,
17 1992). These methods usually attach specific DNA sequences to very small specific areas of
18 a solid support, such as micro-wells of a DNA chip. These hybridization formats are micro-
19 scale versions of the conventional "dot blot" and "sandwich" hybridization systems.

20 The micro-formatted hybridization can be used to carry out "sequencing by
21 hybridization" (SBH) (see M. Barinaga, 253 Science, pp. 1489, 1991; W. Bains, 10
22 Bio/Technology, pp. 757-758, 1992). SBH makes use of all possible n-nucleotide oligomers
23 (n-mers) to identify n-mers in an unknown DNA sample, which are subsequently aligned by
24 algorithm analysis to produce the DNA sequence (R. Drmanac and R. Crkvenjakov,
25 Yugoslav Patent Application No. 570/87, 1987; R. Drmanac et al., 4 Genomics, 114, 1989;
26 Strezoska et al., 88 Proc. Natl. Acad. Sci. USA 10089, 1992; and R. Dramanac and R. B.
27 Crkvenjakov, U.S. Patent No. 5,202,231, April 13, 1993).

28 There are two formats for carrying out SBH. The first format involves creating an
29 array of all possible n-mers on a support, which is then hybridized with the target sequence.
30 The second format involves attaching the target sequence to a support, which is sequentially
31 probed with all possible n-mers. Both formats have the fundamental problems of direct probe
32 hybridizations and additional difficulties related to multiplex hybridizations.

1 Southern, United Kingdom Patent Application GB 8810400, 1988; E. M. Southern et
2 al., 13 Genomics 1008, 1992, proposed using the first format to analyze or sequence DNA.
3 Southern identified a known single point mutation using PCR amplified genomic DNA.
4 Southern also described a method for synthesizing an array of oligonucleotides on a solid
5 support for SBH. However, Southern did not address how to achieve optimal stringency
6 condition for each oligonucleotide on an array.

7 Concurrently, Drmanac et al., 260 Science 1649-1652, 1993, used the second format
8 to sequence several short (116 bp) DNA sequences. Target DNAs were attached to
9 membrane supports ("dot blot" format). Each filter was sequentially hybridized with 272
10 labeled 10-mer and 11-mer oligonucleotides. A wide range of stringency condition was used
11 to achieve specific hybridization for each n-mer probe; washing times varied from 5 minutes
12 to overnight, and temperatures from 0°C to 16°C. Most probes required 3 hours of washing at
13 16°C. The filters had to be exposed for 2 to 18 hours in order to detect hybridization signals.
14 The overall false positive hybridization rate was 5% in spite of the simple target sequences,
15 the reduced set of oligomer probes, and the use of the most stringent conditions available.

16 A variety of methods exist for detection and analysis of the hybridization events.
17 Depending on the reporter group (fluorophore, enzyme, radioisotope, etc.) used to label the
18 DNA probe, detection and analysis are carried out fluorometrically, colorimetrically, or by
19 autoradiography. By observing and measuring emitted radiation, such as fluorescent
20 radiation or particle emission, information may be obtained about the hybridization events.
21 Even when detection methods have very high intrinsic sensitivity, detection of hybridization
22 events is difficult because of the background presence of non-specifically bound materials.

23 In the many applications of DNA hybridization for research and diagnostics, the most
24 difficult analysis involve the differentiation of a single base mismatch from a match target
25 sequence. This is because the analysis involves discriminating a small difference in one
26 hybridized pair, the mismatch, from the match. The teachings of this invention are of
27 particular relevance to these problems.

28 Summary of the Invention

29 As a main aspect of this invention, it has been surprisingly discovered that the
30 fluorescence signal obtained during the electronic denaturation or dehybridization of DNA
31 hybrids is perturbed at or around the electronic power (current and voltage) levels which are

1 associated with the denaturation or dehybridization process. In one embodiment, the
2 fluorescence signal perturbation phenomena appears as a rise or spike in fluorescence
3 intensity prior to dehybridization of a fluorescent labeled probe from a capture sequence
4 attached to the microlocation test site. The power level, amplitude and slope of this
5 fluorescence spike provide analytical tools for diagnosis. The combination of the
6 fluorescence perturbation with other measurements also indicative of the hybridization
7 match/mismatch state, such as consideration of the electronic melting (50% fluorescence
8 decrease during electronic stringency control) can in combination provide a more efficient
9 and reliable hybridization match/mismatch analysis.

10 In general, this controlled dehybridization or electronic stringency process results in a
11 significant differential between the final fluorescent intensity values for the match versus the
12 mismatch sequence. This difference in fluorescent intensity values is used to determine a
13 discrimination ratio, which confirms and identifies that a particular mismatch was present in
14 the sample.

15 It has been discovered that the fluorescent perturbation effect (FPE) provides a
16 powerful analytical tool for DNA hybridization analysis, particularly for the near
17 instantaneous, e.g., less than one minute, and especially less than 5 seconds, discrimination
18 of match/mismatched DNA hybrids. Novel DNA sequencing applications are possible. New
19 fluorescent donor/acceptor/quencher energy transfer mechanisms are created. New electronic
20 catalytic mechanisms are created.

21 In one aspect, this invention relates to using precisely controlled electric or
22 electrophoretic fields to cause or influence fluorophore or chromophore groups in special
23 arrangements with molecular structures (such as nucleic acids), to produce rapid signal
24 variations (perturbations) which correlate with and identify small differences in these
25 molecular structures. In a preferred method for hybridization analysis of a sample, an
26 electronic stringency control device is used to perform the steps of: providing the sample, a
27 first probe with a fluorescent label and a second probe with a label under hybridization
28 conditions on the electronic stringency control device, forming a hybridization product,
29 subjecting the hybridization product to an electric field force, monitoring the fluorescence
30 from the hybridization product, and analyzing the fluorescent signal. The label preferably
31 serves as a quencher for the fluorescent label.

1 Most broadly, this invention relates to integrated microelectronic systems, devices,
2 components, electronic based procedures, electronic based methods, electronic based
3 mechanisms, and flurophore/chromophore arrangements for: (1)molecular biological and
4 clinical diagnostic analyses; (2) nucleic acid sequencing applications; and (3) for carrying out
5 catalysis of biomolecular, organic, and inorganic reactions.

6 More specifically, the molecular biological and clinical diagnostic analyses relate to
7 the utilization of the electronic fluorescent perturbation based mechanisms for the detection
8 and identification of nucleic acid hybrids, single base mismatches, point mutations, single
9 nucleotide polymorphisms (SNPs), base deletions, base insertions, crossover/splicing points
10 (translocations), intron/exon junctions, restriction fragment length polymorphisms (RFLPs),
11 short tandem repeats (STRs) and other repeating or polymorphic sequences in nucleic acids.

12 More specifically, the nucleic acid sequencing applications involve utilization of the
13 electronic fluorescent perturbation based mechanisms to elucidate base sequence information
14 in DNA, RNA and in nucleic acid derivatives. Most particularly, to elucidate sequence
15 information from the terminal ends of the nucleic acid molecules. This method achieves
16 electronic fluorescence perturbation on an electronic stringency control device comprising the
17 steps of: locating a first polynucleotide and a second polynucleotide adjacent the electronic
18 stringency control device, the first polynucleotide and second polynucleotide being
19 complementary over at least a portion of their lengths and forming a hybridization product,
20 the hybridization product having an associated environmental sensitive emission label,
21 subjecting the hybridization product and label to a varying electrophoretic force, monitoring
22 the emission from the label, and analyzing the monitored emission to determine the electronic
23 fluorescence perturbation effect.

24 More specifically, the catalytic reactions relate to the utilization of electronic based
25 catalytic mechanisms for carrying out biomolecular, biopolymer, organic polymer, inorganic
26 polymer, organic, inorganic, and other types of chemical reactions. Additionally, the
27 electronic based catalytic mechanisms can be utilized for carrying out nanofabrication, and
28 other self-assembly or self-organizational processes. This method provides for electronic
29 perturbation catalysis of substrate molecules on an electronic control device containing at
30 least one microlocation comprising the steps of: immobilizing on the microlocation an
31 arrangement of one or more reactive groups, exposing the reactive groups to a solution
32 containing the substrate molecules of interest, and applying an electronic pulsing sequence

1 which causes charge separation between the reactive groups to produce a catalytic reaction on
2 the substrate molecules.

3 More generally, the present invention relates to the design, fabrication, and uses of
4 self-addressable self-assembling microelectronic integrated systems, devices, and
5 components which utilize the electronic mechanisms for carrying out the controlled multi-
6 step processing and multiplex reactions in a microscopic, semi-microscopic and macroscopic
7 formats. These reactions include, but are not limited to, most molecular biological
8 procedures, such as: (1) multiplex nucleic acid hybridization analysis in reverse dot blot
9 formats, sandwich formats, homogeneous/heterogeneous formats, target/probe formats, in-
10 situ formats, and flow cytometry formats; (2) nucleic acid, DNA, and RNA sequencing; (3)
11 molecular biological restriction reactions, ligation reactions, and amplification type reactions;
12 (4) immunodiagnostic and antibody/antigen reactions; (5) cell typing and separation
13 procedures; and (6) enzymatic and clinical chemistry type reactions and assays.

14 In addition, the integrated systems, devices, and components which utilize electronic
15 based catalytic mechanisms are able to carry out biomolecular, biopolymer and other types of
16 chemical reactions: (1) based on electric field catalysis; and/or (2) based on multi-step
17 combinatorial biopolymer synthesis, including, but not limited to, the synthesis of
18 polynucleotides and oligonucleotides, peptides, organic molecules, bio- polymers, organic
19 polymers, mixed biopolymers/organic polymers, two and three dimensional nanostructures,
20 and nanostructures and micron-scale structures on or within silicon or other substrate
21 materials.

22 Additionally, with respect to electronic fluorescent perturbation mechanisms, the
23 present invention relates to unique intermolecular and intramolecular constructs and
24 arrangements of chromophores, fluorophores, luminescent molecules or moieties, metal
25 chelates (complexes), enzymes, peptides, and amino acids, associated with nucleic acid
26 sequences, polypeptide sequences, and/or other polymeric materials. Of particular importance
27 being those constructs and arrangements of fluorophores and chromophores which produce
28 fluorescent energy transfer, charge transfer or mechanical mechanisms which can be
29 modulated or affected by electric or electrophoretic fields to produce fluorescent or
30 luminescent signals which provide information about molecular structure.

31 With respect to the electronic catalytic mechanisms in homogeneous (solution) or
32 heterogeneous (solution/solid support) formats, the present invention relates to unique

1 intermolecular and intramolecular constructs and arrangements of chromophores,
2 fluorophores, luminescent molecules or moities, metal chelates (complexes),enzymes,
3 peptides, and amino acids, nucleophilic molecules or moities, electrophilic molecules or
4 moities, general acid or base calalytic molecules or moities, and substrate binding site
5 molecules and moities, associated with nucleic acid sequences, polypeptide sequences, other
6 biopolymers, organic polymers, inorganic polymers, and other polymeric materials.

7 Additionally, this invention relates to the utilization of electric or electrophoretic
8 fields to induce fluorescent perturbation based mechanisms in arrangements of fluorophores
9 and chromophores in solid state or sol-gel state optoelectronic devices and optical memory
10 materials.

11 It is therefore an object of this invention to provide for methods and systems for
12 improved detection and analysis of biological materials.

13 It is yet a further object of this invention to provide for methods which provide for the
14 rapid and accurate discrimination between matches and mismatches in nucleic acid hybrids.

15 Brief Description of the Drawings

16 Fig. 1A is a plot of the relative fluorescent intensity as a function of applied power
17 (microwatts) for a 20-mer oligomer duplex (100% AP).

18 Fig. 1B is a plot of the relative fluorescent intensity versus applied power
19 (microwatts) for a 19-mer oligomer duplex (53% GC).

20 Fig. 2A is a graph of the relative fluorescent intensity verus applied power
21 (microwatts) for a 20-mer oligomer duplex (100% AT).

22 Fig. 2B is a plot of the relative fluorescent intensity verus applied power (microwatts)
23 for a 19-mer oligomer duplex (53% GC).

24 Fig. 3A shows a cross-sectional view of a mismatched test site having a capture
25 probe, target DNA and a reporter probe.

26 Fig. 3B is a cross-sectional view of target DNA and a reporter probe with an
27 associated fluorophore.

28 Fig. 3C is a graph of the fluorescent response graphing the relative fluorescent
29 intensity as a function of time for a pulses sequence.

30 Fig. 4A is a cross-sectional view of a matched test site having a capture probe, target
31 DNA and a reporter probe with an intercalated fluorophore.

1 Fig. 4B is a cross-sectional view of target DNA and a reporter probe with an
2 intercalating fluorophore.

3 Fig. 4C is a graph of the fluorescent response showing the relative fluorescence
4 intensity as a function of time for a pulsed sequence.

5 Fig. 5 shows the fluorescent intensity (% remaining Fluorescein) profiles as a function
6 of time (seconds) for a one base mismatch and a match sequence for Ras G 22 mers during
7 the basic electronic dehybridization process.

8 Fig. 6 shows the fluorescent intensity (% remaining fluorescence) as a function of
9 time (seconds) observed during the general electronic dehybridization of match/mismatch
10 hybrids for the Ras and RCA5 (HLA)systems.

11 Fig. 7A shows a graph of the normalized fluorescent intensity versus time (seconds)
12 for match/mismatch profiles exhibiting the oscillating fluorescent perturbation effect.

13 Fig. 7B shows an expanded view graph of the first 12 seconds of the graph of Fig. 7A.

14 Fig. 8A shows a schematic representation for the hybridized arrangement of the target
15 probe and the Bodipy Texas Red labeled reporter probe, and the position of the one base
16 mismatch.

17 Fig. 8B shows a schematic representation of Fig. 8A, but where a mismatch between
18 the target and probe is present.

19 Fig. 9 shows a graph of the normalized fluorescent intensity as a function of time
20 (seconds) match/mismatch profiles exhibiting the oscillating fluorescent perturbation effect,
21 in the presence of a second probe containing a quencher group (Malachite Green).

22 Fig. 10A shows a schematic representation for the hybridized arrangement of the
23 target probe, the Bodipy Texas Red labeled reporter probe, and the Malachite Green quencher
24 probe.

25 Fig. 10B shows the schematic representation of Fig. 10A with a mismatch between
26 the target and the probe.

27 Fig. 11A shows a schematic representation for the hybridized arrangement of a target
28 probe, a labeled reporter probe and a quencher probe.

29 Fig. 11B shows the schematic representation of Fig. 11A with a mismatch between
30 the target and probe.

31 Fig. 12 shows a sequence of steps for electronic perturbation catalysis.

1 Detailed Description of the Invention

2 The APEX device as described in the various parent applications has been utilized in
3 novel ways resulting in methods which improve the analytical or diagnostic capabilities of
4 the device. It has been surprisingly discovered that the fluorescent signal is perturbed during
5 the electronic dehybridization of DNA hybrids. This method has particular application to
6 DNA hybridization and single-base mismatch analysis. Specifically, during electronic
7 dehybridization, also known as stringency control or electronic stringency control, a rise or
8 spike in the fluorescence intensity has been observed just prior to the dehybridization of the
9 fluorescent labeled probes from capture sequences attached to the APEX chip pad.

10 Figs. 1A and 1B show the results of electronic denaturation experiments run on an
11 APEX chip having 25 test microlocations with 80 micron diameter utilizing platinum
12 electrodes. For this use, the chip was overlaid with a 1 micron thick avidin/agarose
13 permeation layer. Two 5'-labeled bodipy Texas Red (Ex 590 nm, EM 630 nm) target probes
14 were used in the experiments. The probe of Fig. 1A was a 20 mer (5'-
15 BYTRAAATTTTAATATATAAT-3') containing 100% AT, with a melting temperature
16 (T_m) of 33°C. The probe of Fig. 1B was a 19 mer (5'BYTR-
17 CCACGTAGAACTGCTCATC-3') containing 53% GC, with a melting temperature (T_m) of
18 54°C. (Melting temperature or T_m refers to the temperature at which the dehybridization
19 process is 50% complete). The appropriate complementary biotinylated capture sequences
20 were attached to the avidin/agarose permeation layer over several of the test pads (on the
21 same chip). The capture probe density was ~10⁸ probes per pad. The fluorescent labeled
22 target probes, at a concentration of ~1.0 μM in 50 mM sodium phosphate (pH 7.0), 500 mM
23 NaCl were first hybridized to the attachment probes on the 5580 chips. The chips were then
24 thoroughly washed with 20 mM NaPO₄ (pH 7.0).

25 Electronic denaturation was then carried out by biasing the test pad negative, and
26 increasing the power to the test pad from ~10⁻¹ microwatts (μW) to ~2 x 10² microwatts (μW)
27 over a 90 second time period. Three pads were tested for each of the target probes. The
28 relative change in fluorescent intensity was plotted as a function of the increasing power. In
29 general, the electrophoretic field, force or power necessary to dehybridize a probe from its
30 complementary sequence correlates with the binding energy or T_m (melting temperature) for
31 the DNA duplex. In above experiments the overall power level (μW) necessary to
32 dehybridize the 19-mer probe with 53% GC probe (T_m of 54°C) was higher than for the 20-

mer probe with 100% AT (T_m of 33°C), that is, the equivalent electronic melting point (E_m) at which dehybridization is 50% complete is higher for the 53% GC probe. Also, the fluorescent perturbation (Figs. 1A and 1B, circled region) for the 10-mer probe with 53% GC is observed to be significantly different from that associated with the 100% AT probe.

Figs. 2A and 2B show the results of denaturation experiments run on the APEX chip having 25 test microlocations with 20 micron deep wells to the underlying platinum electrodes. The well structures on the chip were filled with avidin/agarose composite, forming a 20 micron deep permeation layer. The same fluorescent target probes, capture probes and protocols were used in the deep well experiments as in the operation of the device resulting in the information of Figs. 1A and 1B. As in the first experiments, the overall power (μW) necessary to dehybridize the 19-mer probe with 53% GC (T_m of 54°C), is higher than for the 20-mer probe with 100% AT (T_m of 33°C). Also, the slope for the 100% AT probe is much shallower, then for the 53% GC probe. The fluorescent perturbation/spike phenomena is very pronounced for the 19-mer probe with 53% GC in the deep well experiments.

The fluorescent perturbation phenomena correlates well with the sequence specificity of the dehybridization process. The power level (μW) value, amplitude and slope of the fluorescent spike are useful for many aspects of hybridization analysis including single base mismatch analysis. The fluorescent perturbation (F_p) value, namely those values associated with the fluorescence perturbation, e.g., onset value, peak height and slope, combined with the electronic melting (E_m) values, namely, the half-height value of fluorescence, provide significantly higher reliability and additional certainty to hybridization match/mismatch analysis. By combining two or more analytical measurements, a more effective and precise determination may be made.

In the above experiments, the target probes were labeled with a Bodipy Texas Red fluorophore in their 5' terminal positions. While Bodipy TR is not a particularly environmentally sensitive fluorophore it nevertheless showed pronounced effects during electronic denaturation. More environmentally sensitive fluorophores may be used to obtain larger perturbations in their fluorescent properties during electronic dehybridization.

The placement of a sensitive fluorescent label in optimal proximity to the initial denaturation site is preferred. By associating certain fluorescent labels in proximity to the denaturation site, as opposed to labeling at the end of the target or probe, increased specificity

1 and enhanced effects may result. As shown in Fig. 3A and 4A, an intercalating fluorophore
2 10 may be disposed between a reporter probe 2 and target DNA 4. Fig. 3A shows the
3 condition in which the reporter probe 2 is mismatched from the target DNA 4 by a
4 mismatched base 6. In each of Figs. 3A and 4A, the capture probe 8 serves to capture the
5 target DNA 4, with the pad 12 providing the electrophoretic action. Preferably, the
6 intercalating fluorophore 10 would be placed next to the single base mismatch site 6 (Fig.
7 3A). The intercalating type fluorescent label could be, for example, ethidium bromide and
8 acridine derivatives, or any other known fluorescent labels consistent with the objects of this
9 device and its use.

10 Fig. 3B and 4B show the condition of the reporter probe 2, the target DNA 4 and the
11 mismatch base site 6 after the application of a pulse at the fluorescent perturbation value via
12 the pad 12. The change from intercalated to the non-intercalated environment would produce
13 a major change in fluorescent signal intensity for certain labels like ethidium.

14 Furthermore, the use of a mismatch site directed fluorophore label does not require
15 that the hybrid be completely denatured during the process. As shown in Fig. 3C and Fig.
16 4C, an analysis procedure is preferred in which an appropriate pulsed "Fp" power level is
17 applied which causes a mismatched hybridization site to partially denature and renature
18 relative to a matched hybridization site. The procedure results in an oscillating fluorescent
19 signal being observed for mismatch hybrid site, while the fluorescent signal for the matched
20 hybrid site remains unchanged. Figs. 3C and 4C shows the relative fluorescent intensity as a
21 function of varied applied power. This procedure provides a highly specific and
22 discriminating method for single base mismatch analysis. Additional advantages include: (1)
23 longer probes (> 20-mer) than those used in conventional hybridization procedures can be
24 used in this process, (2) Probe specificity is more determined by placement of the fluorescent
25 label (particularly for single base mismatches), and (3) as the procedure does not require
26 complete denaturation of the hybrid structures, each sample can be analyzed repetitively for
27 providing a higher statistical significant data, such as through standard averaging techniques.

28 Referring to Fig. 5, in the process of carrying out electronic DNA hybridization and
29 selective dehybridization (by electronic stringency) on active DNA chip devices (e.g., on an
30 APEX chip), it was surprisingly discovered that the fluorescence signal from labeled reporter
31 probes or target DNAs was perturbed during the initiation of electronic dehybridization at or
32 around the electronic power levels (current and voltage) associated with that dehybridization

1 process. Specifically, this fluorescence signal perturbation shows itself often as a rise or
2 spike in the fluorescence intensity prior to dehybridization of the fluorescent labeled probe
3 sequence from the DNA sequence attached to the microscopic test site (microlocation) on the
4 DNA chip surface. The main region of fluorescence perturbation is shown in the dashed
5 circle.

6 The fluorescent perturbation effect (FPE) is usually most pronounced for a one base
7 mismatched probe sequence relative to the match probe sequence. In the general electronic
8 hybridization and dehybridization procedure, the precisely controlled electronic stringency
9 process results in a significant differential between the final fluorescent intensity values for
10 the match versus the mismatch sequence. The mismatch sequence is more effectively
11 dehybridized and more rapidly removed from the test location than the match sequence. In
12 the general electronic hybridization and dehybridization process this difference in fluorescent
13 intensity values is used to determine a discrimination ratio, which confirms and identifies that
14 a particular mismatch was present in the sample. The particular parameters of electric field
15 strength (current/voltage), solution conductivity, electrode geometry and pulsing time used to
16 produce this selective dehybridization between the match and the mismatch occur at what is
17 called the electronic melting temperature (Etm). The electronic dehybridization and
18 stringency process allows match/mismatch discriminations to be carried out very rapidly
19 (within substantially 20 to 60 seconds), compared with the classical hybridization stringency
20 process, which involves temperature control and stringent washing procedures, which can
21 take hours to complete. The single base pair mismatch (single BPM) sequence is observed to
22 decrease faster than the match sequence allowing one to obtain a match/mismatch
23 discrimination ratio for the pair.

24 Initial observations of the fluorescent perturbation effect (FPE), which occurs almost
25 immediately upon initiation of the electronic dehybridization process, indicated that it was
26 possible to use the FPE as a way to distinguish match/mismatched DNA hybrids even more
27 rapidly, typically in less than a minute, and most preferably in several seconds or less.
28 Another very powerful and novel feature of the FPE is that this technique does not require
29 the removal of the probe or target sequence in order to discriminate a match from the
30 mismatch hybrid, whereas the general electronic dehybridization process and classical
31 hybridization techniques typically require the removal of the mismatch sequence relative to
32 the matched sequence. A further advantage of the FPE technique is that probes of any size

1 can potentially be used for match/mismatch hybrid discriminations or other applications.
2 Longer probes sequences can provide overall better hybridization stability and selectivity.

3 Further investigations of the fluorescent perturbation effect has revealed other aspects
4 and advantages of this unique phenomena which include: (1) that the amplitude, frequency,
5 and slope of this fluorescent signal can provide a powerful analytical tool for other types of
6 DNA hybridization analysis, in addition to the near instantaneous discrimination of single
7 base mismatched DNA; (2) that multiple probe systems, involving a quencher probe and
8 fluorescent acceptor probe (and donor probes), can be used to further enhance the FPE
9 technique; (3) that a variety of electronic pulsing sequences (DC and AC variations) can be
10 developed which further improve and broaden the scope of FPE based analysis of DNA and
11 other molecular structures; (4) that the electronic fluorescence perturbation mechanism could
12 lead to DNA sequencing applications; (5) that new arrangements of fluorescent
13 donor/acceptor/quencher groups could be created for improved energy transfer mechanisms
14 and applications; and (6) that novel electronic catalytic mechanisms could be created. These
15 are the subjects of this invention.

16 The basic fluorescent perturbation effect occurs generally upon the initiation of
17 electronic denaturation of match and mismatch hybrid pairs. In the case of the Ras (ras
18 oncogene) hybrids in Fig. 5, the mismatch nucleotide is located approximately in the middle
19 of the probe sequence, and the fluorescent label (Bodipy Texas Red) is covalently attached to
20 the terminal position of the oligonucleotide sequence, approximately 10 bases from the
21 mismatched nucleotide (see Example 1, below). Upon initiation of dehybridization process
22 the fluorophore responds to the changing environment of the dehybridizing DNA strands by
23 brightening. Generally, most fluorophores are somewhat sensitive to their local physical,
24 chemical, and thermal environments; and a number of fluorophores are found to be extremely
25 sensitive to changes in their environment. Environmental parameters such as hydrophilicity,
26 hydrophobicity, pH, electrostatic charge, and Van der Waals interactions, can cause changes
27 in the fluorescent intensity (quantum yield), the excitation/emission spectrum, and/or the
28 fluorescent life time. Many of these environmental parameters are believed to change due to
29 some or all of: (1) the disruption of the double-stranded DNA structure; (2) the effect of a DC
30 or AC electric field and/or the electrophoretic effects on the fluorophore itself; (3) the effect
31 of a DC or AC electric field and/or the electrophoretic effects on the fluorophore/DNA
32 structure, which has its own unique set of interactions that can depend upon base

1 sequence(AT or GC rich areas), and whether the fluorophore is associated with a double or
2 single-stranded form of the nucleic acid; and/or (3) changes in the local electrochemical
3 environment. It does appear that initial destabilization of the double-stranded structure is
4 most important to the process. This is because the effect on the mismatch is more pronounced
5 than for the match, both of which are present in the same general environment.

6 It is believed that the subtle fluorophore/DNA structural interactions are also very
7 important. This is the basis for DNA sequencing techniques disclosed herein.

8 Fig. 6 shows some further examples of the fluorescent perturbation effect observed
9 during the general electronic dehybridization and stringency process for match/mismatch
10 hybrids for the Ras and RCA5 (HLA)systems (see Example 2, below). The effect again is
11 observed for both the Ras and RCA5 mismatch sequences, being particularly pronounced for
12 RCA5 hybrid pair.

13 In general electronic hybridization and stringency experiments, the reporter or target
14 probes are typically labeled with a Bodipy Texas Red fluorophore in their 5' (or 3')terminal
15 positions. While Bodipy TR is not a particularly environmentally sensitive fluorophore it
16 nevertheless showed pronounced effects during electronic dehybridization process. More
17 environmentally sensitive fluorophores may be used to obtain larger perturbations in their
18 fluorescent properties during FPE process. By way of example, these fluorophores and
19 chromophores include: other Bodipy dye derivatives, ethidiums (in particular derivatized
20 forms of ethidium dyes which can be covalently attached to DNA), or other intercalating
21 fluorophores (which are or can be derivatized for attachment to DNA, acridines, fluoresceins,
22 rhodoamines, Texas Red (sulforhodamine 101), Cy3 and Cy5 dyes, Lucifer Yellow, and
23 Europium and Terbium chelate dye derivatives, IR144 and far red laser dyes and derivatives.
24 Other fluorophores, chromophores and dyes consistent with the methods and objects of these
25 inventions may be utilized.

26 In general, any dye which is sensitive to the environmental parameters such as
27 hydrophilicity, hydrophobicity, pH, electrostatic charge, Van der Waals interactions, etc., that
28 can cause changes in the fluorescent intensity (quantum yield), the excitation/emission
29 spectrum, and/or the fluorescent life time, are potentially useful for FPE applications. More
30 particularly useful, are those fluorophores, chromophores, or dyes which have properties
31 which change or are perturbed due to the following.

1 (1) The initial disruption or destabilization of the double-stranded DNA structure.
2 This is optionally just near the terminal position of the DNA structure where the fluorophore
3 is located.

4 (2) The effects of the DC or AC electric field (or electrophoretic field) on the
5 fluorophore itself. Of importance would be whether the fluorophore is neutral or charged,
6 and whether the net charge is positive or negative. The net charge could strongly influence
7 the perturbation effect, particularly if the fluorophore were positively charged. In this case,
8 the fluorophore would tend to move in an opposite direction relative to the rest of the DNA
9 molecule when an electric field is applied.

10 (3) The effect of the DC or AC electric field (or electrophoretic field) on the
11 fluorophore/DNA interaction itself. Again, whether the fluorophore was neutral, net positive,
12 or net negatively charged would have a pronounced effect on the nature and stability of the
13 fluorophore/DNA interaction.

14 (4) The general spectral properties and robustness of the dye are also important. For
15 example, the excitation and emission maxima, the Stokes shift, and the resistance to fading
16 under excitation conditions are also important. Of particular usefulness would be those dyes
17 which have excitation maxima at or above 480 nm, and emissions at or above 520 nm, and
18 Stokes shifts of more than 20 nm. More useful, would be those dyes which have excitation
19 maxima at or above 590 nm, and emissions at or above 620 nm, and Stokes shifts of more
20 than 20 nm. Most useful, would be those dyes which have excitation maximum at or above
21 650 nm, and emissions at or above 670 nm, and Stokes shifts of more than 20 nm.

22 The placement of a sensitive fluorophore or chromophore label or reporter in optimal
23 proximity to the initial destabilization or base mismatch site is important for achieving the
24 electronic fluorescent perturbation effect (FPE). The preferred arrangements would be to
25 have the fluorophore or chromophore within 0 to 10 bases of the initial destabilization or base
26 mismatch site. The most preferred arrangements would be to have the fluorophore or
27 chromophore within 0 to 5 bases of the initial destabilization or base mismatch site.

28 It should be kept in mind, that when a fluorophore or chromophore group is at the
29 terminal position (5' or 3') of a DNA sequence which is hybridized to a complementary
30 sequence, the group is already located in some sense at a "destabilized" site relative to the
31 rest of the hybridized structure. This is because the terminal or end positions of a hybrid
32 structure are less stable (the strands are opening and closing or fraying) relative to the internal

1 hybridized sequence. One important aspect of this invention is to design the probe sequences
2 such that they now position the further destabilizing base mismatch nucleotide site (in the
3 target or probe sequence), so that upon hybridization the base mismatch is in closer proximity
4 to the terminal fluorophore or chromophore group or groups. By associating the
5 destabilization site in closer proximity to the terminal fluorophore or chromophore group(s),
6 it is possible to utilize electronic pulsing sequences which produce fluorescent perturbation
7 effects which correlate well with molecular structure, i.e., detect and identify point mutations,
8 base deletions, base insertion, nucleotide repeat units, and other features important to DNA
9 analysis.

10 Additional advantages to the FPE technique include: (1) the ability to utilize longer
11 probes (> 20-mer) than those used in conventional hybridization procedures, (2) that probe
12 specificity can be determined by placement of the fluorophore or chromophore label
13 (particularly for single base mismatches), and (3) FPE technique does not require
14 dehybridization or removal of the mismatched probe sequence from the system; therefore,
15 each sample can be analyzed repetitively providing a higher statistical significant to data,
16 such as through signal averaging techniques.

17 Most particularly, this invention relates to using precisely controlled AC or DC
18 electric fields or electrophoretic fields to affect or influence fluorophore or chromophore
19 groups in special arrangements with molecular structures (such as nucleic acids), to produce
20 rapid signal variations (perturbations) which correlate with and identify small differences in
21 these molecular structures.

22 Most broadly, this invention relates to integrated microelectronic systems, devices,
23 components, electronic based procedures, electronic based methods, electronic base
24 mechanisms, and fluorophore/chromophore arrangements for: (1) molecular biological and
25 clinical diagnostic analyses; (2) nucleic acid sequencing applications; and (3) for carrying out
26 catalysis of biomolecular, organic, and inorganic reactions.

27 More specifically, the molecular biological and clinical diagnostic analyses relate to
28 the utilization of the electronic fluorescent perturbation based mechanisms for the detection
29 and identification of nucleic acid hybrids, single base mismatches, point mutations, single
30 nucleotide polymorphisms (SNPs), base deletions, base insertions, crossover/splicing points
31 (translocations), intron/exon junctions, restriction fragment length polymorphisms (RFLPs),

1 short tandem repeats (STRs) and other repeating or polymorphic sequences in nucleic acid
2 acids.

3 More specifically, the nucleic acid sequencing applications involve utilization of the
4 electronic fluorescent perturbation based mechanisms to elucidate base sequence information
5 in DNA, RNA, and in nucleic acid derivatives. Most particularly, to elucidate sequence
6 information from the terminal ends of the nucleic acid molecules.

7 More specifically, the catalytic reactions relate to the utilization of electronic based
8 catalytic mechanisms for carrying out biomolecular, biopolymer, organic polymer, inorganic
9 polymer, organic, inorganic, and other types of chemical reactions. Additionally, the
10 electronic based catalytic mechanisms can be utilized for carrying out nanofabrication, and
11 other self-assembly or self-organizational processes. More generally, the present invention
12 relates to the design, fabrication, and uses of self-addressable self-assembling microelectronic
13 integrated systems, devices, and components which utilize the electronic mechanisms for
14 carrying out the controlled multi-step processing and multiplex reactions in a microscopic,
15 semi-microscopic and macroscopic formats. These reactions include, but are not limited to,
16 most molecular biological procedures, such as: (1) multiplex nucleic acid hybridization
17 analysis in reverse dot blot formats, sandwich formats, homogeneous/heterogeneous formats,
18 target/probe formats, and in-situ formats, and flow cytometry formats; (2)nucleic acid, DNA,
19 and RNA sequencing; (3) molecular biological restriction reactions, ligation reactions, and
20 amplification type reactions; (4)immunodiagnostic and antibody/antigen reactions; (5)cell
21 typing and separation procedures; and (6)enzymatic and clinical chemistry type reactions and
22 assays.

23 In addition, the integrated systems, devices, and components which utilize electronic
24 based catalytic mechanisms are able to carry out biomolecular, biopolymer and other types of
25 chemical reactions: (1) based on electric field catalysis; and/or (2)based on multi-step
26 combinatorial biopolymer synthesis, including, but not limited to, the synthesis of
27 polynucleotides and oligonucleotides, peptides, organic molecules, biopolymers, organic
28 polymers, mixed biopolymers/organic polymers, two and three dimensional nanostructures,
29 and nanostructures and micron-scale structures on or within silicon or other substrate
30 materials.

31 Additionally, with respect to electronic fluorescent perturbation mechanisms, the
32 present invention relates to unique intermolecular and intramolecular constructs and

1 arrangements of chromophores, fluorophores, luminescent molecules or moities, metal
2 chelates (complexes),enzymes, peptides, and amino acids, associated with nucleic acid
3 sequences, polypeptide sequences, and/or other polymeric materials. Of particular importance
4 being those constructs and arrangements of fluorophores and chromophores which produce
5 fluorescent energy transfer, charge transfer or mechanical mechanisms which can be
6 modulated or affected by the AC or DC electric fields or electrophoretic fields to produce
7 fluorescent or luminescent signals which provide information about molecular structure.

8 With respect to the electronic catalytic mechanisms in homogeneous (solution) or
9 heterogeneous (solution/solid support) formats, the present invention relates to unique
10 intermolecular and intramolecular constructs and arrangements of chromophores,
11 fluorophores, luminescent molecules or moities, metal chelates (complexes),enzymes,
12 peptides, and amino acids, nucleophilic molecules or moities, electrophilic molecules or
13 moities, general acid or base catalytic molecules or moities, and substrate binding site
14 molecules and moities, associated with nucleic acid sequences, polypeptide sequences, other
15 biopolymers, organic polymers, inorganic polymers, and other polymeric materials.

16 Additionally, this invention relates to the utilization of electric or electrophoretic
17 fields to induce fluorescent perturbation based mechanisms in arrangements of fluorophores
18 and chromophores in solid state or sol-gel state optoelectronic devices and optical memory
19 materials.

20 FPE With A Single Fluorophore

21 Fig. 7A shows a graph of the normalized match/mismatch profiles exhibiting the
22 oscillating fluorescent perturbation effect for a probe with a single fluorescent reporter group.
23 A pronounced difference is observed between the match and the mismatch hybrids. The
24 match and mismatch hybrid pairs have the mismatched nucleotide located two bases from the
25 Bodipy Texas Red fluorescent reporter group which is attached to the 3'-terminal position of
26 the reporter probe. The x-axis of the graph is seconds, and the y-axis is relative fluorescent
27 intensity units. The electronic pulse sequence used was 500 nA for 0.5 seconds on/0.75
28 second off, run for 30 seconds (see Example 3). In this example the match and mismatch
29 hybrid pairs have the mismatched nucleotide located two bases from the Bodipy Texas Red
30 fluorescent reporter group which is attached to the 3'-terminal position of the reporter probe.

Fig. 7B now shows an expanded view graph of the first 12 seconds for the normalized match/mismatch profiles exhibiting the oscillating fluorescent perturbation effect. A very pronounced difference is observed in the first few seconds after the pulse sequence is initiated, after which the match and the mismatch continue to oscillate at different amplitudes. It is believed that the higher amplitude oscillation by the match is due to the faster and more efficient rehybridization by the fully complementary (match) sequence relative to a non-fully complementary sequence (mismatch). This faster “snap-back” of the match relative to the mismatch may be used to distinguish those cases. Fig. 7B shows that the upon initiation of the DC pulse sequence that the fluorescent intensity for the mismatch rises rapidly, while the fluorescent intensity for the match actually decreases momentarily. The mismatch and the match then seem to come into phase, but oscillate at different amplitudes. It is such pronounced differences which allow the FPE to be used to differentiate between the match and mismatched DNA structures.

Figs. 8A and 8B show a schematic representation for the hybridized arrangement of the target probe and the Bodipy Texas Red labeled reporter probe, and the position of the one base mismatch (Fig. 8B). The mismatched nucleotide is located two bases from the Bodipy Texas Red fluorescent reporter group which is attached to the 3'-terminal position of the reporter probe. The most preferred arrangements for carrying out FPE techniques with a single fluorophore would be to have it located within 0 to 5 bases of the mismatched location (see Example 3, below).

FPE With Multiple Fluorophore/Chromophore Arrangements

Fig. 9 shows a graph of the normalized match/mismatch profiles exhibiting the oscillating fluorescent perturbation effect, in the presence of a second probe containing a quencher group (Malachite Green). A pronounced difference is observed between the match and the mismatch hybrids upon application of the electric field. There is immediately a very large increase in fluorescent intensity due to the loss of the quenching effect upon initiation of the electric field. After the “de-quenching” the match and the mismatch continue to oscillate at different amplitudes. This represent just one example of how a unique fluorophore/chromophore arrangement can be used to enhance or improve the FPE technique. Additionally, this represents an example of how a unique energy transfer or quenching mechanism can be designed, which responds to a DC pulsing electric field (electrophoretic

1 field), and produces a unique fluorescent response (a dramatic increase in intensity). It is also
2 disclosed in this invention, that AC electric fields (including high frequencies > 100 Hz),
3 would have fluorescent perturbation effects which would be useful for analysis of molecular
4 structures, in particular for DNA hybridization analysis.

5 In the example shown in Fig. 9, the match and mismatch hybrid pairs have the
6 mismatched nucleotide located two bases from the Bodipy Texas Red fluorescent reporter
7 group, which is attached to the 3'-terminal position of the reporter probe. The second probe
8 (quencher probe) hybridizes to the target sequence in such a way that it positions the
9 Malachite Green quencher group (attached at the 5'-terminal position) within three bases of
10 the Bodipy Texas Red fluorophore group on the 3'-terminal position of the reporter probe.
11 Upon hybridization, the quencher probe causes about a 40-50% decrease in the fluorescent
12 intensity of the Bodipy Texas Red reporter (which is eliminated when the electric field is
13 applied). Other arrangements and quencher chromophores could produce even better
14 quenching and reduction of fluorescence from the reporter group. In Fig. 9, the x-axis of the
15 graph is in seconds, and the y-axis is in relative fluorescent intensity units. The electronic
16 pulse sequence used was 600 nA for 1.0 seconds on/1.5 second off, run for 30 seconds (see
17 Example 4, below).

18 Figs. 10A and 10B show a schematic representation for the hybridized arrangement of
19 the target probe, the Bodipy Texas Red labeled reporter probe, and the Malachite Green
20 quencher probe. The mismatched nucleotide (Fig. 10B) is located two bases from the
21 fluorescent reporter group (Bodipy Texas Red) located on the terminal position of the
22 reporter probe. The second probe (quencher probe) hybridizes to the target sequence in such
23 a way that it positions the Malachite Green quencher group (attached at the 5'-terminal
24 position) within three bases of the Bodipy Texas Red fluorophore group on the 3'-terminal
25 position of the reporter probe. Other useful fluorophore/chromophore forms and
26 arrangements would include those in which the quencher probe is designed to be hybridized
27 within 0 to 5 bases of the mismatch position.

28 Of particular usefulness for this invention is one of the preferred arrangement shown
29 in Figs. 11A and 11B. In this example, the first probe (a capture/quencher probe sequence)
30 has two terminal functional groups, a 5'-terminal biotin group which allows the probe to be
31 immobilized to the surface (permeation layer) of a microlocation test site on an active DNA
32 chip or other hybridization device. The second functional group being a quencher group, (such

1 as Malachite Green, Reactive Red, or other quencher chromophore), which is at the 3'-
2 terminal position of the capture/quencher probe. The capture/quencher probes are made
3 complementary to the match and mismatch point mutation sequences of interest. These
4 probes allow the target DNA (RNA) sequence to be captured by selective hybridization and
5 immobilized on the microlocation test site. The sequence is designed to optimally position the
6 (potential) mismatched nucleotide within one to five bases of the quencher group. After the
7 hybridization/capture of the target DNA (RNA) sequence, the second probe (acceptor
8 reporter) is added and hybridized to the immobilized target DNA/quencher probe. The
9 acceptor/reporter probe is labeled in its 5'-terminal position with a suitable fluorophore
10 (Bodipy Texas Red, or other reporter group), and designed to hybridize to the target DNA
11 sequence in such a way as to be optimally positioned within 1 to 5 bases of the quencher
12 group, where upon hybridization the acceptor reporter groups fluorescence is quenched.
13 Upon application of the appropriate electronic DC pulsing sequence (current/on time/off
14 time)an electric field is induced which causes the match and mismatched hybrids to produce a
15 fluorescent perturbation effect and oscillations which allow them to be distinguished and
16 identified. It should be pointed out that the above hybridization procedure could also be
17 carried out in a semi-homogeneous format, in which the target DNA sequence is first
18 hybridized in solution with the reporter probe sequence, before hybridization to the
19 immobilized capture/quencher probe. The above describes just some of the potentially useful
20 formats for PFE. It is important to realize that flexibility in choosing various FPE techniques
21 and formats will be advantageous for successful broad area hybridization diagnostics. The
22 scope of this invention also includes the utilization of the FPE processes described above, in
23 highly multiplexed formats on APEX DNA chips and array devices.

24 Additionally, the scope of this invention includes the use and incorporation of various
25 donor/acceptor/quencher, mechanisms, probe arrangements and hybridization formats which
26 were described in our photonic patents (U.S. Patent No. 5,532,129 and U.S. Patent No.
27 5,565,322) and optical memory application (WO 95/34890). The novel electronic pulsing
28 scenarios combined with the donor/acceptor/quencher arrangements described in the above
29 applications leads to useful FPE quenching and energy transfer mechanism, which further
30 enhance and expand the usefulness of the techniques for DNA hybridization and other
31 molecular analysis.

1 Electronic Perturbation Catalysis

2 The discovery of the fluorescent perturbation effect has also contributed to the further
3 discovery of a way to carry out novel electronic perturbation catalysis. In particular it lead to
4 discovering a way to over come what is called the leaving group effect in enzyme catalysis.
5 Investigators trying to create synthetic enzyme-like catalysts have not been able to overcome
6 this obstacle . (see M.J. Heller, J.A. Walder, and I.M. Klotz, Intramolecular Catalysis of
7 Acylation and Deacylation in Peptides Containing Cysteine and Histidine, J. American
8 Chemical Society, 99, 2780, 1997).

9 Fig. 12 shows a diagram of a peptide structure containing an arrangement of
10 nucleophilic groups (cysteine-thiol and histidine-imidazole) designed to carry out electronic
11 perturbation catalysis, ester hydrolysis and deacylation in particular. Two examples of such
12 cysteine and histidine containing peptide structures include: Gly-His-Phe-Cys-Phe-Gly and
13 Gly-His-Pro-Cys-Pro-Gly. In the example shown in Fig. 12, a cysteine (thiol) and histidine
14 (imidazole) containing catalytic peptide sequence is immobilized onto the surface
15 (permeation layer) of a microlocation on an active electronic device (via the terminal alpha
16 amino group). The system is designed to catalyze the cleavage of esters and amide bonds
17 (Step 1). The catalytic peptide/device is exposed to a solution containing the particular
18 substrate of interest (ester, amide, etc.), which hydrolyzes and forms an acyl-thiol
19 intermediate (Steps 1 and 2). In general, the acyl-thiol group will not deacylate even when the
20 imidazole group is in close proximity, because of the back attack between the two
21 nucleophiles (Step 3). Electronic perturbation catalysis is carried out by applying an
22 appropriate electronic pulsing sequence (current, on time/off time), which causes charge
23 separation between the negatively charged thiol group and the positively charged acyl-
24 imidazole group (Step 4), allowing the acyl-imidazole group to effectively deacylate before
25 the thiol group can re-attack (Step 5). The system is now ready to catalyze the hydrolysis of
26 a new substrate molecule (Step 6). This example represent just one of many possible
27 catalytic arrangements and applications for electronic perturbation catalysis.

28 EXPERIMENTAL RESULTS

29 Example 1 - Ras G Match/Mismatch

30 APEX Chip Preparation and Capture Probe Loading - APEX active DNA chips, with
31 25 microlocation test sites (80 microns in diameter) were coated with streptavidin agarose

1 accordingly. A 2.5% glyoxal agarose (FMC) solution in water was made according to
2 manufacturer's instructions. The stock was equilibrated at 65°C, for 5 minutes. Chips were
3 spin coated at 2.5K rpm for 20 seconds. Another layer was then applied at 10K rpm for 20
4 seconds. This second "thin layer was composed of a 1:4 mix of 5mg/ml streptavidin (BM) in
5 50mM NaPhosphate, 250mM NaCl and 2.5% glyoxal agarose.

6 The chips were baked at 37°C for 30 minutes. Streptavidin was coupled to the
7 agarose via Schiff's base reduction in 0.1M NaCNBH3 in 0.3M NaBorate, pH 9.0, for 60
8 minutes, at room temperature. The remaining aldehydes were capped with 0.1M glycine, for
9 30 minutes, at room temperature, and finally rinsed in water, dried under N₂ and then stored
10 at 4°C.

11 The table below gives the sequence and labeling positions for all the oligonucleotide
12 probes and target sequences used in examples 1 and 2. Mismatches are underlined and
13 bolded.

14

<u>Name</u>	<u>Sequence (5'-3')</u>	<u>Modification</u>	<u>Modified</u> <u>end</u>
Ras 411	GCCCACACCGCCGGCGCCCACC	Bodipy Texas Red	5'
Ras 415	GGTGGGCGCCGGCGGTGTGGGC	Biotin	5'
Ras 416	GGTGGGCGCCGG <u>A</u> GGTGTGGGC	Biotin	5'
HLA 253	CCACGTAGAACTGCTCATC	Bodipy Texas Red	5'
HLA 241	GATGAGCAGTTCTACGTGG	Biotin	3'
HLA 378	GATGAGCAG <u>C</u> TCTACGTGG	Biotin	3'
HLA 375	<u>T</u> ATGAGCAGTTCTACGTGG	Biotin	3'
HLA 376	GATGAGCAGTTCTACGT <u>T</u>	Biotin	3'

HLA 401 GATGAGCAGTTCTACGTGG

Biotin

5'

1 Capture Probe Addressing for Example 1 - Columns 1 & 2 on the APEX chip were
2 electronically addressed with the Ras 415 (match) sequence and columns 4 & 5 loaded with
3 Ras 416 (mismatch) sequence. Addressing was carried out in 50mM cysteine, 1M
4 oligonucleotide, 200 nA for 1 min. The target/reporter sequence Ras 411 was passively
5 hybridized in 500mM NaCl, 50mM NaPhosphate pH 7.4, at room temperature for 5 minutes).
6 Electronic dehybridization and stringency was done at 1.5 μ A/microlocation, DC pulsing for
7 0.1 sec on, 0.2 sec off, 150 cycles (20 mM NaPhosphate, pH 7.4). Microlocations were
8 given electronic stringency individually. Fluorescence signal was captured at 1 second
9 intervals. Normalized displayed is the average of three test sites for each point. Error bars are
10 standard deviations. Results are shown in Fig. 5.

11 Example 2 - Ras G and HLA Match/Mismatches

12 The APEX chip preparation procedure was the same as Example 1. Capture probe
13 addressing conditions were the same as Example 1. The Ras 415 sequence was electronically
14 addressed to all 5 microlocations in column 1 and Ras 416 addressed to all 5 microlocations
15 in column 2 of the APEX chip. The HLA 241 sequence was addressed to all 5
16 microlocations in column 4 and HLA 378 was addressed to all 5 microlocations in column 5.
17 The Ras 411 and HLA 253 fluorescent target probes were mixed and passively hybridized to
18 the APEX chip. Electronic dehybridization and stringency was carried out for the Ras system
19 at 1.5 μ A/microlocation, DC pulsing for 0.1 sec on, 0.2 sec off, 150 cycles (20 mM
20 NaPhosphate, pH 7.4). Electronic dehybridization and stringency for the HLA system was
21 carried out at 0.6 μ A /microlocation, DC pulsing for 0.1 sec on, 0.2 sec off, 150 cycles (20
22 mM NaPhosphate, pH 7.4). Data collected as reported above. Fig. 6 shows the results for
23 Example 2.

24 Example 3 - Fluorescent Perturbation Effect With Single Fluorophore

25 APEX Chip Preparation and Capture Probe Loading - APEX active DNA chips, with
26 25 microlocation test sites (80 microns in diameter) were coated with streptavidin agarose
27 accordingly. A 2.5% glyoxal agarose (FMC) solution in water was made according to

1 manufacturer's instructions. The stock was equilibrated at 65°C, for 5 minutes. Chips were
2 spin coated at 2.5K rpm for 20 seconds. Another layer was then applied at 10K rpm for
3 20seconds. This second "thin layer was composed of a 1:4 mix of mg/ml streptavidin (BM)
4 in 50mM NaPhosphate, 250mM NaCl and 2.5% glyoxal agarose. The chips were baked at
5 37°C for 30 minutes. Streptavidin was coupled to the agarose via Schiff's base reduction in
6 0.1M NaCNBH₃ in 0.3M NaBorate, pH 9.0, for 60 minutes, at room temperature. The
7 remaining aldehydes were capped with 0.1M glycine, for 30 minutes, at room temperature,
8 and finally rinsed in water, dried under N₂ and then stored at 4°C.

9 The sequences for the oligonucleotide reporter probe, quencher probe and capture
10 probe used in Examples 3 and 4 are listed below:

11 QATAR-1 (perfect match for reporter and quencher)

12 5'-biotin-CAC gAg AgA CTC ATg AgC Agg ggC TAg CCg ATC ggg TCC TCA ggT CAA
13 gTC

14 QATAR-2

15 5'-biotin-CAC gAg AgA CTC ATg AgC Agg (C)gC TAg CCg ATC ggg TCC TCA ggT
16 CAA gTC

17 QATAR-3A (1 base mismatch)

18 5'-biotin-CAC gAg AgA CTC ATg AgC Agg ggC TAg CC(A) ATC ggg TCC TCA ggT
19 CAA gTC

20 QATAR-4A (2 base mismatch)

21 5'-biotin-CAC gAg AgA CTC ATg AgC Agg ggC TAg CC(A) A(C)C ggg TCC TCA ggT
22 CAA gTC

23 QATAR-5A (perfect match to reporter, no quencher hybridization)

24 5'-biotin-gCA CCT gAC TCC TgA ggA gAA gTC CCg ATC ggg TCC TCA ggT CAA gTC

25 ET60-BODIPY TR (Reporter)

26 5'-TgA CCT gAg gAC CCg ATC g - BODIPY TR

27 ET71-Malachite Green (Quencher)

28 5'-malachite green - Ag CCC CTg CTC ATg AgT CTC T

1 The capture probes were addressed to specific microlocation test sites (pads) on the
2 APEX chip as follows: a 10 μ l aliquot containing 500nM capture probe in 50 mM histidine
3 buffer was applied to the chip and positive bias was applied at 200nA/pad, for 30 seconds.
4 The bias was turned off and the chip was fluidically washed in 50mM histidine. QATAR-1
5 was addressed to column 1, QATAR-3A was addressed to column 2, QATAR-4A was
6 addressed to column 3, and QATAR-5 was addressed to column 4.

7 Hybridization and Quenching Efficiency

8 The addressed APEX chips were passively hybridized with ET60-BTR reporter
9 with/without ET71-MG quencher at 500nM each in 100mM NaPhosphate, at pH 7.2, 250mM
10 NaCl, at 65°C in a heat block, for 2 minutes. The chips were washed in 20mM NaPhosphate,
11 pH 7.2, at room temperature, 3 times for 10 minutes each wash.

12

Capture	Reporter ET60-BTR	Quencher ET71-MG
QATAR-1	match	match
QATAR-3A	1 base pair mismatch	match
QATAR-4A	2 base pair mismatch	match
QATAR-5	match	none

13

14 Comparison of hybridization signal intensities indicated that fluorescent quenching
15 was about 50% efficient. This could be improved with optimized spacing and or increased
16 purification of the probes (higher specific activity).

17 Fluorescence Perturbation for Reporter Probe Only

18 The chips were mounted on a probe station with a probe card to provide electrical
19 contact to the chip, waveforms were supplied by Keithley Power Supply, images acquired
20 via Optronics cooled color CCD and NIH image software was used to analyze the data. The
21 preferred imaging system is that disclosed in copending U.S. Application entitled "Scanning
22 Optical Detection System", filed May 1, 1997, incorporated herein by reference as if fully set
23 forth herein.

24 Chips were prepared and hybridized as described in Example 1 and 2. In 20mM
25 NaPhosphate, pH 7.2, individual pads were biased negative and a pulse waveform was
26 applied. Parameters tested were pulse frequency, %duty cycle, and amplitude. Good

1 fluorescence perturbation results were observed at 600nA/1 sec On/1.5 sec Off. The camera
2 integration was 1.0 second. Higher pulse frequencies could also be effective but these
3 experiments were limited by the amount of fluorescence at each pad location which
4 necessitated longer camera integration times.

5 Results from the perfect match reporter/quencher pair on QATAR 1 showed approx
6 10% increase in fluorescence intensity when the power was first applied and the intensity
7 oscillated during the course of the waveform. On QATAR-5 which did not have the
8 quencher hybridized there was very little fluorescence perturbation. Both QATAR 3a and 4a
9 some fluorescence perturbation but not as much as QATAR1. Additionally, signal loss after
10 bias was greatest for QATAR-4A, followed by 3A, followed by 5 and then 1. This would be
11 expected based on the hybrid Tm's. The results for QATAR-1 (match) and the QATAR-3
12 (mismatch) are shown in Figs. 7A and 7B.

13 Example 4: Fluorescence Perturbation With Reporter and Quencher Probes

14 APEX chips were prepared and hybridized as described in Examples 1, 2, and 3.
15 Microlocation test sites were biased as in Example 3 except that the CCD camera integration
16 was 0.5 seconds. Results showed that QATAR-1 produced approximately 60% increase in
17 fluorescence intensity when power first applied and intensity oscillated during the entire
18 waveform. For QATAR-5, which did not have the quencher when hybridized, there was very
19 little fluorescence perturbation. Both QATAR 3A and 4A showed an initial increase in
20 fluorescence approaching 40%. There was a significant decrease in intensity on QATAR-4A
21 after bias applied. This is indicative of the lower Tm of this hybrid which had 2 mismatches.
22 The results for QATAR 1 (match) and QATAR 3 (mismatch) are shown in Fig. 9.

23 Although the foregoing invention has been described in some detail by way of
24 illustration and example for purposes of clarity and understanding, it may be readily apparent
25 to those of ordinary skill in the art in light of the teachings of this invention that certain
26 changes and modifications may be made thereto without departing from the spirit or scope of
27 the appended claims.